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Elsevier Editorial System(tm) for Archives of Physical Medicine and Rehabilitation Manuscript Draft

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Title: Feedback device for improvement of coordination of reach-to-grasp following stroke

Article Type: Brief Report

Keywords: Stroke, Physical Therapy, Feedback, Equipment and Supplies

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Abstract:

Abstract

Title: Feedback device for improvement of coordination of reach-to-grasp following stroke

Objective

To describe a novel feedback device (GRASP) that gives feedback about the time lag between the start of hand opening and the start of the transport during reach-to-grasp movements and to report the results of a preliminary series of single case studies to assess the utility of the device for improving the coordination of arm and hand at the beginning of a reach-to-grasp movement.

Design

A multiple baseline design across six subjects was used, with each subject performing forty repetitions of reaching to grasp a jar. Two subjects each performed 10, 15, or 20 randomly assigned baseline repetitions.

Setting Physiotherapy department or at the participant's home.

Participants

Six participants with middle cerebral artery or parietal stroke were consecutively recruited from physiotherapy departments. Additional inclusion criteria were a Rivermead Motor Assessment score of 5 or more and time between start of hand opening and transport more than 60 ms.

Interventions

During the intervention phase, feedback on time between start of transport and start of grasp was communicated via GRASP. Participants were encouraged to reduce the time.

Main outcome measures

The outcome measure was the time between start of transport and start of grasp, measured with GRASP.

Results

All participants decreased the mean time lag during the intervention phase compared to the baseline phase. Participants 1 to 6 showed decreases of 35, 296, 34, 34, 1212 and 114 milliseconds respectively. Two out of six participants demonstrated a significant decrease of time lag in the intervention compared to the baseline phase.

Conclusions

GRASP is potentially beneficial as an adjunct to physiotherapy training of reach-to-grasp coordination after stroke.

Key words

Stroke, Physical Therapy, Feedback, Equipment and Supplies

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8th July, 2011

Dear Dr Rogers,

This is a resubmission of a manuscript with the title '**Feedback device for improvement of coordination of reach-to-grasp following stroke',** manuscript number ARCHIVES-PMR-D-11-00621.

Thank you for your email requesting minor revision of this Brief Report. The required changes have now been made to the manuscript, and a separate document itemising the response to each reviewer comment has been attached.

Changes to the manuscript have been highlighted in yellow.

Many thanks for your further consideration of this manuscript.

Yours sincerely

Paulette van Vliet

Ms. Ref. No.: ARCHIVES-PMR-D-11-00621

Title: Feedback device for improvement of coordination of reach-to-grasp following stroke

Archives of Physical Medicine and Rehabilitation

Itemised Responses to reviewer comments

| Reviewer Comment | Response |
|---|---|
| ABSTRACT | |
| Better wording: "A multiple baseline design across six subjects was used, with each subject performing forty repetitions of reaching to grasp a jar." Two subjects each performed 10, 15, or 20 randomly assigned baseline repetitions." | Design section of abstract has been changed to : "A multiple baseline design across six subjects was used, with each subject performing forty repetitions of reaching to grasp a jar. Two subjects each performed 10, 15, or 20 randomly assigned baseline repetitions." |
| INTRODUCTION Line 25preliminary multiple baseline design across six subjects to assess Line 66the following multiple baseline design. | Line 25 is now line 86 and has been changed to: "to report the results of a preliminary multiple baseline design across six subjects to assess the utility of the device" Line 66 is now line 127 and has been changed to: "the following multiple baseline design." |
| METHODS 69 DELETE | Line 69 is now line 130 and heading 'SINGLE CASE STUDIES' deleted. |
| 94 A multiple baseline design across six subjects was conducted with each subject completing 40 trials. | Line 94 is now line 155 and is changed to: "A multiple baseline design across six subjects was conducted with each subject completing 40 trials." |
| 96-97 A multiple baseline approach was used to decrease. | Line 96-97, now line 157-158 is changed to: "A multiple baseline approach was used to decrease" |
| RESULTS Please add "levels" to Figure 1. | A line for each "level" (mean) in each phase has been added to Figure 1. |

| DISCUSSION DISCUSSION is true to the RESULTS Because the changes are in milliseconds, the authors need to address the "so what" question. Are the changes "functional" and "meaningful" ? | The following has been inserted into the discussion, lines 246-249. "The improved temporal coordination in participants 2, 5 and 6 indicates that this aspect of the motor control of reach to grasp was executed in a more normal way. This is a meaningful change, as improvements in motor control are |
|---|---|
| DISCUSSION Study limitations: Following resubmission of the manuscript, the editorial office suggested adding a 'study limitations' subheading, and some wording about limitations. | likely to lead to improved arm function." Lines 250-254 of the discussion have been changed to: "These preliminary findings provide valuable data on the utility of our prototype. Study limitations Due to the small sample size, the results cannot be generalised to a wider population. The next step will be a controlled clinical trial with a larger group, to test whether GRASP as an adjunct to reach-to-grasp training yields better outcomes than reach-to-grasp training alone." |

Running Head: Feedback device for arm movements in stroke

Title Page

Title: Feedback device for improvement of coordination of reach-to-grasp following stroke

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Word count main text: 2098 Word count abstract: 274 Figures: 2 Tables: 1

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We certify that no party having a direct interest in the results of the research supporting this article has or will confer a benefit on us or on any organization with which we are associated AND, if applicable, we certify that all financial and material support for this research (eg, NIH or NHS grants) and work are clearly identified in the title page of the manuscript.

The device(s) that is/are the subject of this manuscript is/are not FDA-approved and is/are not commercially available in the United States.

The work described in this manuscript was supported by a Spinner Pathfinder grant.

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| 54 | SELV | - | Separated extra-low voltage |
| 55 | IEE | - | Institution of Electrical Engineers |
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Following stroke, only 20% to 56% ¹ of people regain useful upper limb function after three months. New technologies to assist more people to regain useful arm movement would therefore have major benefits. An important motor impairment resulting from stroke is a lack of coordination between arm and hand ^{2 3}. This brief report evaluates a feedback device that can be used to improve the coordination of arm and hand at the beginning of a reach-to-grasp movement.

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In the reach-to-grasp of healthy subjects, an invariant temporal relationship exists
between transport and grasp components ⁴. The start time of the hand opening is
correlated with the start of hand movement towards the object, and the time of maximum
hand opening is correlated with the time of peak deceleration of the hand ⁴. Stroke ^{3 5},
especially involving the middle cerebral artery (MCA) ² can cause difficulties with this
temporal coordination.

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Feedback about the time between the start of hand opening and the start of transport
could be used to direct the participant's efforts to timing these events to start together,
thereby inducing a more normal temporal coordination of reach-to-grasp. Currently no
feedback devices perform this function for reach-to-grasp, though feedback devices can
improve performance of other body movements ⁶.

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83 This report aims to (a) describe a device called 'GRASP' – 'grasp rehabilitation

84 accessory for stroke participants'- that gives feedback to both participant and therapist

85 about the time lag between the start of hand opening and the start of the transport and (b)

| 86 | to report the results of a preliminary multiple baseline design across six subjects to |
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| 90 | DEVICE DESCRIPTION |
| 91 | The device (Figure 1) comprises (1) sensors to detect the start of both hand opening and |
| 92 | hand transport; (2) a timer measuring the time elapsed between these events; and (3) a |
| 93 | user interface communicating the lapsed time. |
| 94 | |
| 95 | INSERT FIGURE 1 ABOUT HERE |
| 96 | |
| 97 | Both sensors are touch sensors comprising contact electrodes configured to monitor the |
| 98 | electrical conductivity of a user's body through the skin surface. The hand opening |
| 99 | sensor comprises a thumb electrode with a metallic outer surface such that placing a |
| 100 | forefinger into contact initiates a grasp-closed condition. The sensor is activated when |
| 101 | the forefinger moves away from the thumb sensor such that there is loss of contact. This |
| 102 | activates timing. The wrist sensor comprises a metallic base plate, on which the hand |
| 103 | rests, which detects gross contact of a user's lower arm or wrist when at rest. This |
| 104 | sensor is activated when the hand moves away from the base plate. This loss of contact |
| 105 | from the second sensor stops the timer. The resulting time between the two events is |
| 106 | displayed to the user via a visual number display ('Interval (ms) in Figure 1). During the |
| 107 | movement, a wristband worn on the resting arm, holds the electrical potential of the |
| 108 | user's body at a local system ground. |
| | |

| 110 | The two electrodes and wristband are connected by leads to the control unit. The thumb |
|-----|--|
| 111 | electrode is a copper ring with an insulated plastic inner surface. Several sizes are |
| 112 | available to comfortably fit over an adult thumb. The wrist electrode comprises a circular |
| 113 | stainless steel base plate of a size to accommodate an adult user's wrist and hand when in |
| 114 | a loose fist. The wristband is an elasticised bracelet of the type used widely in the |
| 115 | electronics industry as a static grounding system. The materials are stainless steel and |
| 116 | plastic and can be cleaned with alcohol or soapy water. Any danger of electric shock is |
| 117 | removed by using a low and isolated internal source voltage (12 V) complying with |
| 118 | SELV as defined by IEE Regulations – 16 Edition. Such voltages are considered |
| 119 | universally hazard free. A patent application, containing further details, has been |
| 120 | published ⁷ . |
| 121 | |
| 122 | Communication of the lapsed time enables instant feedback on the correlation of the two |
| 123 | events and therefore on their coordination at the start of the movement. It also allows |

124 successive movements to be compared and the temporal order of the movements to be

seen, i.e. whether the hand opened or moved forward first.

- 126
- Preliminary data of the utility of the device was collected within the following multiplebaseline design.
- 129
- 130 **Participants**
- 131 Stroke participants were recruited consecutively from physiotherapy outpatient
- 132 departments. Testing took place at the participants' location inpatient or outpatient

| 133 | physiotherapy department, or at home. The local Research Ethics Committee and |
|------------|--|
| 134 | Medicines and Healthcare products Regulatory Agency approved all procedures. |
| 135 | Inclusion criteria were: MCA or parietal stroke, a score of 5 or more on the arm section |
| 136 | of the Rivermead Motor Assessment (Reach forward, pick up large ball with both hands |
| 137 | and place down again) and 'time between start of hand opening and start of hand |
| 138 | transport > 60 ms' (exceeds normal limits). Exclusion criteria were: cognitive |
| 139 | dysfunction which prevented understanding of the task, severe concurrent medical |
| 140 | problems that prevent repetitive reaching (including shoulder pain), lack of informed |
| 141 | consent. Six stroke participants took part consisting of 2 women and 4 men, with a mean |
| 142 | age of 48.2 years (SD 14.6) and time since event causing brain damage was 22.1 months |
| 143 | (SD 19.2). None had receptive but two had expressive communication difficulties. |
| 144 | Participant characteristics are shown in Table 1. In summary, none had receptive or |
| 145 | expressive communication difficulties, the group had a moderate degree of arm |
| 146 | impairment, minor increases in muscle tone apart from participant 6, minor |
| 147 | proprioception loss except for participant 3, minimal presence of neglect, optic ataxia, |
| 148 | and impairments of spatial perception. |
| 149 150 | |
| 151 | |
| 152 | |
| 153 | |
| 154 | Design |
| 155 | A multiple baseline design across six subjects was conducted with each subject |
| 156 | completing 40 trials. An AB design was used because the participants' performance was |

157 not expected to revert to baseline after withdrawal of the intervention. A multiple

158 baseline approach was used to decrease the likelihood of extraneous variables causing a

159 change from baseline to intervention phase – an effect would be demonstrated if the

160 measure changed only when the intervention is introduced. The baseline phase consisted

161 of a randomly assigned length of 10, 15 or 20 repetitions, two participants performing

162 each length. This was followed by a series of intervention trials, numbering 30, 25 or 20

trials, depending on the number of repetitions in the baseline phase.

164 *Procedure*

165 Two research physiotherapists not involved with the design of GRASP conducted these 166 studies. Participants reached to grasp a glass jar (height 92mm, diameter 70 mm, weight

167 230g), placed 30 cm anterior to the starting position of the hand, and moved it onto a

round mat (14 cm diameter) on the table, placed closer to the body (5 cm in front of start

169 position). The hand started directly in front of the elbow, with the jar directly ahead of the

170 hand so that no change in shoulder rotation was required to grasp the jar. At the start, the

171 finger was touching the thumb sensor, the forearm was in mid-pronation, the elbow was

172 at 100 degrees flexion, and the wrist rested on the metal plate, positioned along the edge

173 of the table. The other arm rested in the participant's lap. Instructions were "reach

174 forward, pick up the jar, and place it on the mat".

175 During baseline, the device was attached and performance was recorded but no feedback

176 was given. During the intervention phase, feedback was given. The following instructions

177 ensued at the beginning of the intervention phase:

178 "When reaching to grasp an object, the start of your hand opening and the start of your

arm movement forwards, usually occur at the same time, i.e. they are synchronised.

Some people with stroke have difficulty with this synchronisation. This machine is 181 designed to give you feedback to make these two events more synchronised. 182 The display will tell you the time, in number of milliseconds, between the two events. 183 Your aim is to try to make this number as small as possible, by thinking about making the 184 start of the hand opening and the start of arm movement forward, happen at the same 185 time".

186

180

187 Then the required number of trials was performed for the intervention phase. After each 188 trial, the participant observed the result shown on the display, which indicated the time 189 between the start of hand transport and start of grasp, in milliseconds, and which of these 190 components started first.

191

192 Data analysis

193 The outcome measure was the time between start of hand transport and start of grasp 194 (time lag), measured in milliseconds by GRASP. This was recorded for each of the 40 195 trials of each of the participants and depicted graphically for visual inspection (Figure 2). 196 Mean time lag in each of the baseline and intervention phases were calculated. To 197 determine whether there was a significant difference between time lag results during 198 baseline and intervention phases, the two-standard deviation band method, described by Nourbaksh and Ottenbacher (1994)⁸ was used. Following the method as described by 199 200 Nourbaksh and Ottenbacher, the standard deviation is computed for the baseline data, 201 then bands are drawn on the graph that contain scores within ± 2 standard deviations 202 from the mean. A significant difference is considered to have occurred if 'at least two

successive data points in the intervention phase fall outside the two-standard deviation
band^{*8}. This procedure has the advantage of 'being sensitive to changes in the variability
across phases of a single-subject design^{*8}.

206

207 RESULTS

208 Visual inspection of results

209 Results are shown graphically in Figure 2. On visual inspection, participant 3 showed an

210 increasing time lag during Phase A, the baseline, followed by a decreasing time lag

211 during Phase B, the intervention. The remaining five participants demonstrated a

212 decreasing time lag already during Phase A, the baseline phase. The time lag of

213 participants 2 and 5 continued to decrease in the intervention phase. For participants 1

and 4 however, there was a trend towards increasing the time lag in the intervention

215 phase. Participant 5 demonstrated an uncharacteristically large time lag on the second

trial of the baseline phase (5559 ms). This value was atypical as all other values for other

217 subjects were below 1410ms. "

218

219 Statistical analysis

220 All participants decreased the mean time lag during intervention compared to baseline

221 (Figure 2). Mean decreases in time lag between phases within each participant were, for

participants 1 through to 6 respectively: 35, 296, 34, 34, 1212 and 114 milliseconds.

223 Participants 2 and 6 showed a significant decrease of time lag in the intervention

compared to the baseline phase, using the two-standard deviation band method.

225 Participant 5 did not show a significant decrease of time lag in the intervention compared

| 226 | to the baseline phase, when the atypical value was included. However, we hypothesised |
|-----|--|
| 227 | that the reason for this atypical value which occurred on only the second trial, was that |
| 228 | this participant's performance was initially affected by a lack of familiarity with the task |
| 229 | and the device and for this reason the analysis was repeated with this value was removed |
| 230 | from the analysis, leaving 9 baseline trials instead of 10. In this case, there was a |
| 231 | significant decrease of time lag in the intervention compared to the baseline phase. |
| 232 | Participants 1, 3 and 6 did not show a significant difference between the phases. |
| 233 | |
| 234 | INSERT FIGURE 2 ABOUT HERE |
| 235 | |
| 236 | DISCUSSION |
| 237 | Several participants were able to use the feedback to continue to significantly reduce the |
| 238 | time lag between the start of transport and the start of grasp and there was a reduction in |
| 239 | mean time lag in the intervention phase compared to the baseline phase for all |
| 240 | participants. Thus GRASP could act as a useful adjunct to current physiotherapy |
| 241 | intervention for coordination. Participants 2, 5 and 6 benefited most and two of these (2 |
| 242 | and 6) were earlier after stroke and with less motor impairment than other participants, so |
| 243 | GRASP may be of greater benefit to people in this group. However, three of these |
| 244 | participants did not show that GRASP demonstrated an additional effect to that of |
| 245 | practising the task. |
| 246 | The improved temporal coordination in participants 2, 5 and 6 indicates that this aspect of |
| 247 | the motor control of reach to grasp was executed in a more normal way. This is a |

- 248 meaningful change, as improvements in motor control are likely to lead to improved arm
- 249 **function.** These preliminary findings provide valuable data on the utility of our prototype.
- 250 Study limitations
- 251 Due to the small sample size, the results cannot be generalised to a wider population. The
- 252 next step will be a controlled clinical trial with a larger group, to test whether GRASP as
- an adjunct to reach-to-grasp training yields better outcomes than reach-to-grasp training
- 254 alone.
- 255 CONCLUSION
- 256 This preliminary investigation of GRASP indicates that it is potentially beneficial as an
- adjunct to physiotherapy training of reach-to-grasp function after stroke.

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 Nourbaksh MR, Ottenbacher KJ. The statistical analysis of single-subject data: a comparative examination. *Physical Therapy* 1994;74(8). Figure 1 GRASP ready to record a reaching movement

Figure 2. Results for baseline (Phase A) and intervention phase (Phase B) for participants 1 to 6. The vertical line denotes the start of phase B. Trial number is shown on the horizontal axis and time between start of hand transport and start of grasp (ms) is shown on the vertical axis. Mean time lag values are shown for each phase. The 2 standard deviation bands above and below the mean are also indicated. Negative standard deviation bands are not shown as there were no negative values. Mean levels are also shown by horizontal lines in each phase.

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| 102 | activates timing. The wrist sensor comprises a metallic base plate, on which the hand |
| 103 | rests, which detects gross contact of a user's lower arm or wrist when at rest. This |
| 104 | sensor is activated when the hand moves away from the base plate. This loss of contact |
| 105 | from the second sensor stops the timer. The resulting time between the two events is |
| 106 | displayed to the user via a visual number display ('Interval (ms) in Figure 1). During the |
| 107 | movement, a wristband worn on the resting arm, holds the electrical potential of the |
| 108 | user's body at a local system ground. |
| | |

| 110 | The two electrodes and wristband are connected by leads to the control unit. The thumb |
|-----|--|
| 111 | electrode is a copper ring with an insulated plastic inner surface. Several sizes are |
| 112 | available to comfortably fit over an adult thumb. The wrist electrode comprises a circular |
| 113 | stainless steel base plate of a size to accommodate an adult user's wrist and hand when in |
| 114 | a loose fist. The wristband is an elasticised bracelet of the type used widely in the |
| 115 | electronics industry as a static grounding system. The materials are stainless steel and |
| 116 | plastic and can be cleaned with alcohol or soapy water. Any danger of electric shock is |
| 117 | removed by using a low and isolated internal source voltage (12 V) complying with |
| 118 | SELV as defined by IEE Regulations – 16 Edition. Such voltages are considered |
| 119 | universally hazard free. A patent application, containing further details, has been |
| 120 | published ⁷ . |
| 121 | |
| 122 | Communication of the lapsed time enables instant feedback on the correlation of the two |
| 123 | events and therefore on their coordination at the start of the movement. It also allows |

124 successive movements to be compared and the temporal order of the movements to be

seen, i.e. whether the hand opened or moved forward first.

- 126
- Preliminary data of the utility of the device was collected within the following multiplebaseline design.
- 129
- 130 **Participants**
- 131 Stroke participants were recruited consecutively from physiotherapy outpatient
- 132 departments. Testing took place at the participants' location inpatient or outpatient

| 133 | physiotherapy department, or at home. The local Research Ethics Committee and |
|------------|--|
| 134 | Medicines and Healthcare products Regulatory Agency approved all procedures. |
| 135 | Inclusion criteria were: MCA or parietal stroke, a score of 5 or more on the arm section |
| 136 | of the Rivermead Motor Assessment (Reach forward, pick up large ball with both hands |
| 137 | and place down again) and 'time between start of hand opening and start of hand |
| 138 | transport > 60 ms' (exceeds normal limits). Exclusion criteria were: cognitive |
| 139 | dysfunction which prevented understanding of the task, severe concurrent medical |
| 140 | problems that prevent repetitive reaching (including shoulder pain), lack of informed |
| 141 | consent. Six stroke participants took part consisting of 2 women and 4 men, with a mean |
| 142 | age of 48.2 years (SD 14.6) and time since event causing brain damage was 22.1 months |
| 143 | (SD 19.2). None had receptive but two had expressive communication difficulties. |
| 144 | Participant characteristics are shown in Table 1. In summary, none had receptive or |
| 145 | expressive communication difficulties, the group had a moderate degree of arm |
| 146 | impairment, minor increases in muscle tone apart from participant 6, minor |
| 147 | proprioception loss except for participant 3, minimal presence of neglect, optic ataxia, |
| 148 | and impairments of spatial perception. |
| 149 150 | |
| 151 | |
| 152 | |
| 153 | |
| 154 | Design |
| 155 | A multiple baseline design across six subjects was conducted with each subject |
| 156 | completing 40 trials. An AB design was used because the participants' performance was |

157 not expected to revert to baseline after withdrawal of the intervention. A multiple

158 baseline approach was used to decrease the likelihood of extraneous variables causing a

159 change from baseline to intervention phase – an effect would be demonstrated if the

160 measure changed only when the intervention is introduced. The baseline phase consisted

161 of a randomly assigned length of 10, 15 or 20 repetitions, two participants performing

162 each length. This was followed by a series of intervention trials, numbering 30, 25 or 20

trials, depending on the number of repetitions in the baseline phase.

164 *Procedure*

165 Two research physiotherapists not involved with the design of GRASP conducted these 166 studies. Participants reached to grasp a glass jar (height 92mm, diameter 70 mm, weight

167 230g), placed 30 cm anterior to the starting position of the hand, and moved it onto a

round mat (14 cm diameter) on the table, placed closer to the body (5 cm in front of start

169 position). The hand started directly in front of the elbow, with the jar directly ahead of the

170 hand so that no change in shoulder rotation was required to grasp the jar. At the start, the

171 finger was touching the thumb sensor, the forearm was in mid-pronation, the elbow was

172 at 100 degrees flexion, and the wrist rested on the metal plate, positioned along the edge

173 of the table. The other arm rested in the participant's lap. Instructions were "reach

174 forward, pick up the jar, and place it on the mat".

175 During baseline, the device was attached and performance was recorded but no feedback

176 was given. During the intervention phase, feedback was given. The following instructions

177 ensued at the beginning of the intervention phase:

178 "When reaching to grasp an object, the start of your hand opening and the start of your

arm movement forwards, usually occur at the same time, i.e. they are synchronised.

Some people with stroke have difficulty with this synchronisation. This machine is 181 designed to give you feedback to make these two events more synchronised. 182 The display will tell you the time, in number of milliseconds, between the two events. 183 Your aim is to try to make this number as small as possible, by thinking about making the 184 start of the hand opening and the start of arm movement forward, happen at the same 185 time".

186

180

187 Then the required number of trials was performed for the intervention phase. After each 188 trial, the participant observed the result shown on the display, which indicated the time 189 between the start of hand transport and start of grasp, in milliseconds, and which of these 190 components started first.

191

192 Data analysis

193 The outcome measure was the time between start of hand transport and start of grasp 194 (time lag), measured in milliseconds by GRASP. This was recorded for each of the 40 195 trials of each of the participants and depicted graphically for visual inspection (Figure 2). 196 Mean time lag in each of the baseline and intervention phases were calculated. To 197 determine whether there was a significant difference between time lag results during 198 baseline and intervention phases, the two-standard deviation band method, described by Nourbaksh and Ottenbacher (1994)⁸ was used. Following the method as described by 199 200 Nourbaksh and Ottenbacher, the standard deviation is computed for the baseline data, 201 then bands are drawn on the graph that contain scores within ± 2 standard deviations 202 from the mean. A significant difference is considered to have occurred if 'at least two

successive data points in the intervention phase fall outside the two-standard deviation
band^{*8}. This procedure has the advantage of 'being sensitive to changes in the variability
across phases of a single-subject design^{*8}.

206

207 RESULTS

208 Visual inspection of results

209 Results are shown graphically in Figure 2. On visual inspection, participant 3 showed an

210 increasing time lag during Phase A, the baseline, followed by a decreasing time lag

211 during Phase B, the intervention. The remaining five participants demonstrated a

212 decreasing time lag already during Phase A, the baseline phase. The time lag of

213 participants 2 and 5 continued to decrease in the intervention phase. For participants 1

and 4 however, there was a trend towards increasing the time lag in the intervention

215 phase. Participant 5 demonstrated an uncharacteristically large time lag on the second

trial of the baseline phase (5559 ms). This value was atypical as all other values for other

217 subjects were below 1410ms. "

218

219 Statistical analysis

220 All participants decreased the mean time lag during intervention compared to baseline

221 (Figure 2). Mean decreases in time lag between phases within each participant were, for

participants 1 through to 6 respectively: 35, 296, 34, 34, 1212 and 114 milliseconds.

223 Participants 2 and 6 showed a significant decrease of time lag in the intervention

compared to the baseline phase, using the two-standard deviation band method.

225 Participant 5 did not show a significant decrease of time lag in the intervention compared

| 226 | to the baseline phase, when the atypical value was included. However, we hypothesised |
|-----|--|
| 227 | that the reason for this atypical value which occurred on only the second trial, was that |
| 228 | this participant's performance was initially affected by a lack of familiarity with the task |
| 229 | and the device and for this reason the analysis was repeated with this value was removed |
| 230 | from the analysis, leaving 9 baseline trials instead of 10. In this case, there was a |
| 231 | significant decrease of time lag in the intervention compared to the baseline phase. |
| 232 | Participants 1, 3 and 6 did not show a significant difference between the phases. |
| 233 | |
| 234 | INSERT FIGURE 2 ABOUT HERE |
| 235 | |
| 236 | DISCUSSION |
| 237 | Several participants were able to use the feedback to continue to significantly reduce the |
| 238 | time lag between the start of transport and the start of grasp and there was a reduction in |
| 239 | mean time lag in the intervention phase compared to the baseline phase for all |
| 240 | participants. Thus GRASP could act as a useful adjunct to current physiotherapy |
| 241 | intervention for coordination. Participants 2, 5 and 6 benefited most and two of these (2 |
| 242 | and 6) were earlier after stroke and with less motor impairment than other participants, so |
| 243 | GRASP may be of greater benefit to people in this group. However, three of these |
| 244 | participants did not show that GRASP demonstrated an additional effect to that of |
| 245 | practising the task. |
| 246 | The improved temporal coordination in participants 2, 5 and 6 indicates that this aspect of |
| 247 | the motor control of reach to grasp was executed in a more normal way. This is a |

- 248 meaningful change, as improvements in motor control are likely to lead to improved arm
- 249 **function.** These preliminary findings provide valuable data on the utility of our prototype.
- 250 **Study limitations**
- 251 Due to the small sample size, the results cannot be generalised to a wider population. The
- 252 next step will be a controlled clinical trial with a larger group, to test whether GRASP as
- an adjunct to reach-to-grasp training yields better outcomes than reach-to-grasp training
- 254 alone.
- 255

256 CONCLUSION

- 257 This preliminary investigation of GRASP indicates that it is potentially beneficial as an
- adjunct to physiotherapy training of reach-to-grasp function after stroke.
- 259

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 Nourbaksh MR, Ottenbacher KJ. The statistical analysis of single-subject data: a comparative examination. *Physical Therapy* 1994;74(8). Figure 1 GRASP ready to record a reaching movement

Figure 2. Results for baseline (Phase A) and intervention phase (Phase B) for participants 1 to 6. The vertical line denotes the start of phase B. Trial number is shown on the horizontal axis and time between start of hand transport and start of grasp (ms) is shown on the vertical axis. Mean time lag values are shown for each phase. The 2 standard deviation bands above and below the mean are also indicated. Negative standard deviation bands are not shown as there were no negative values. Mean levels are also shown by horizontal lines in each phase.

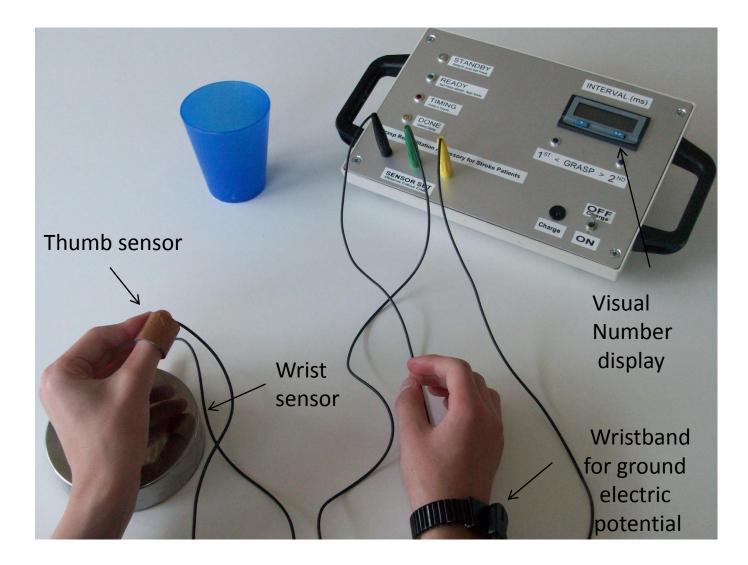
 Table 1. Characteristics of participants

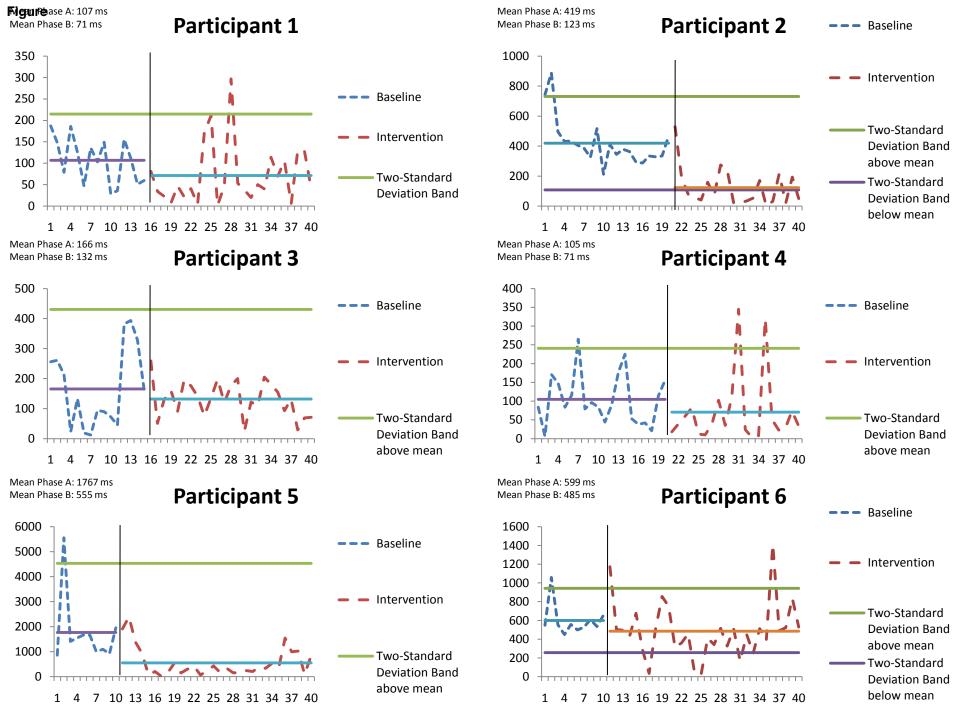
| Participant | CT scan | Time | Arm | Muscle | Neglect | Spatial | Optic | Proprioception |
|-------------|-----------------|----------|----------|----------|---------|------------|--------|----------------|
| no. | result | since | function | tone | § | perception | ataxia | (wrist, |
| | | stroke | * | (wrist, | | | П | finger, |
| | | (months) | | finger, | | | | elbow) # |
| | | | | elbow) † | | | | |
| 1 | Right middle | 14 | 10 | 1,0,1 | 55 | 36 | 35 | 3,2,2 |
| | cerebral | | | | | | | |
| | artery infarct | | | | | | | |
| 2 | Right middle | 8 | 11 | 1,1,0 | 54 | 27.5 | 35 | 2,0,2 |
| | cerebral | | | | | | | |
| | artery infarct, | | | | | | | |
| | particulary | | | | | | | |
| | parieto- | | | | | | | |
| | temporal | | | | | | | |

| | junction and | | | | | | | |
|---|----------------|----|----|-------|----|----|----|-------|
| | internal | | | | | | | |
| | capsule | | | | | | | |
| 3 | Left fronto- | 21 | 5 | 0,0,0 | 54 | 24 | 39 | 2,3,3 |
| | parietal | | | | | | | |
| | infract | | | | | | | |
| 4 | Left Parietal | 17 | 12 | 0,0,1 | 55 | 30 | 36 | 3,3,3 |
| | intracranial | | | | | | | |
| | haemorrhage | | | | | | | |
| 5 | Left middle | 9 | 11 | 0,0,1 | 55 | 31 | 39 | 3,2,3 |
| | cerebral | | | | | | | |
| | infarct | | | | | | | |
| 6 | Left middle | 64 | 5 | 1,3,3 | 55 | 34 | 35 | 3,3,3 |
| | cerebral | | | | | | | |
| | artery infarct | | | | | | | |
| | | | | | | | | |

• * Arm function (Rivermead Motor Assessment) maximum score, 15.

- † Muscle tone (Modified Ashworth Scale) score range: 0, no increase in muscle tone; 4, affected part rigid in flexion or extension.
- § Neglect (star cancellation) normal scoring range, 51-54; spatial perception (Rey figure copy) normal scoring range, 31-36.
- \prod optic ataxia (adapted from the 'reaching for an object' test described by Perenin⁸: maximum score, 40).
- # Proprioception (Nottingham Sensory Assessment) score range: 0, no appreciation of movement; 1, appreciates movement takes place but direction incorrect; 2, mirror the direction of the test movement, but it inaccurate in its new position; 3, Accurately mirrors the test movement to within 10° of the new test position





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